LOCOMOTION CONTROL FOR MANY-MUSCLE HUMANOIDS

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Human Movements

- •Complex musculoskeletal system
- •Coordination of muscle activation

Why Many-Muscles?

Lee et al. 2010 Wang et. al. 2012 Geijtenbeek et. al. 2013

•Enough for complex movements?

Goal

- •Controlling locomotion with complex musculoskeletal system
	- Arbitrarily many (100+) muscles
- •Predicting new gait patterns under varied conditions
	- Pathologic gait patterns

Related Work - Biped Control

Kwon et al. 2010

Yin et al. 2007

Wang et al. 2009

Lasa et al. 2010

Wu et al. 2010

Brown et al. 2013

Al Borno et al. 2013

Lee et al. 2010

Mordatch et al. 2010

Coros et al. 2010

Sok et al. 2007

Muico et al. 2009

Liu et al. 2012

Related Work - Biped Control

FSM / Simple Models

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Motion Capture Data

Zordan et. al. 2004 Lee & Terzopoulos 2006 Sueda et. al. 2008 Lee et. al. 2009

Anderson & Pandy 1999 Thelen et. al. 2003 Thelen et. al. 2006 Nakamura et. al. 2004

Wang et. al. 2012 Geijtenbeek et. al. 2013

Specific Body Parts

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Musculoskeletal Analysis

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Locomotion Control & Synthesis

Challenges of Many-Muscle Control

- Underdetermined system (muscle redundancy)
	- # muscles > # total DOFs
	- Multiple sets of _ muscle forces Same joint torque

- What is best motion for a given situation? (adaptability)
- Complexity of muscle contraction dynamics
	- **Integrated controller design**

Our Approach

•Find optimal muscle actuation considering nonlinear muscle dynamics

•**Seamlessly integrating muscle dynamics into QP formulation** •*Muscle optimization*

Our Approach

•Gait adaptation under various conditions

•**Finding best motion for given condition by offline optimization**

•*Trajectory optimization*

Musculoskeletal Models

Delp et al. 1990; Anderson and Pandy 1999 Steele and Hamner 2013

Gait2562 (25 DOFs, 62 muscles)

Gait2592 (25 DOFs, 92 muscles)

Fullbody (39 DOFs, 120 muscles)

Muscle Activation

- CE : contractile element
- PE : passive element
- α: pennation angle

SE : serial element **CE : contractile element PE : passive element** α: pennation angle

- PE : passive element
- **α: pennation angle**

Muscle Force Generation

 $f_{mt} = (f_{ce} + f_{pe})cos(\alpha)$

 \rightarrow $i = f(a, l)$

Many-Muscle Control

•Muscle optimization • Optimal muscle activation under physics laws & muscle dynamics

•Trajectory optimization • Modulates reference motion for robustness & adaptability

Many-Muscle Control

- •Muscle optimization
	- Optimal muscle activation under physics laws & muscle dynamics
	- *Per-frame tracking simulation*
- •Trajectory optimization
	- Modulates reference motion for robustness & adaptability
	- •*Offline modulation*

Muscle Optimization

 $\ddot{\mathbf{q}}$ λ \mathbf{a} • Finds best (muscle activation, acceleration, contact force) to follow reference motion.

• Muscle activation - resolving muscle redundancy.

• Acceleration & contact force - optimal results under physics laws.

• Reference motion is adjusted by balance strategy by [Kwon & Hodgins 2010].

•Objective

$\|\mathbf{a}\|^2$ **Effort** Contact force **Tracking** End-Effectors

$$
\|\mathbf{x}\|^{2}
$$

$$
\|\ddot{\mathbf{q}}_{d} - \ddot{\mathbf{q}}\|^{2}
$$

$$
\|\ddot{\mathbf{y}}_{d}^{i} - \ddot{\mathbf{y}}^{i}\|^{2} \quad i \in \{\text{left foot, right foot, torso}\}\
$$

•Objective

- $\|\mathbf{a}\|^2$ **Effort** $\|\boldsymbol{\lambda}\|^2$ Contact force $\|\ddot{\mathbf{q}}_d-\ddot{\mathbf{q}}\|^2$ **Tracking** $\|\ddot{\mathbf{y}}_d^i - \ddot{\mathbf{y}}^i\|^2$ End-Effectors
	- $i \in \{$ left foot, right foot, torso $\}$
- Inequality Constraints $f = \lambda_1 v_1 + \lambda_2 v_2 + \lambda_3 v_3 + \lambda_4 v_4$ f $\boldsymbol{\lambda} \geq 0$ $V₂$ Friction cone $V₃$ V_{1} $C(q)\ddot{q} + d(q, \dot{q}) \ge 0$ Non-penetration $V₄$ $0 \le a \le 1$ Muscle activation

Equality Constraint - Equation of Motion

$M(q)\ddot{q} + c(q, \dot{q}) =$ (muscle force) + (contact force)

Equality Constraint - Equation of Motion

$M(q)\ddot{q} + c(q, \dot{q}) =$ (muscle force) + (contact force)

$\mathbf{M}(\mathbf{q})\ddot{\mathbf{q}} + \mathbf{c}(\mathbf{q},\dot{\mathbf{q}}) = \mathbf{G}(\mathbf{q},\mathbf{l})(\mathbf{A}(\mathbf{l},\dot{\mathbf{l}})\mathbf{a} + \mathbf{p}(\mathbf{l},\dot{\mathbf{l}})) + \mathbf{H}(\mathbf{q})\boldsymbol{\lambda}$

.

.

.

Quadratic Programming

minimize
$$
w_1 \|\mathbf{a}\|^2 + w_2 \|\mathbf{\lambda}\|^2 + w_3 \|\ddot{\mathbf{q}}_d - \ddot{\mathbf{q}}\|^2 + \sum_i w_4^i \|\ddot{\mathbf{y}}_d^i - \ddot{\mathbf{y}}^i\|^2
$$

subject to $\mathbf{M}(q)\ddot{q} + c(q, \dot{q}) = \mathbf{G}(q, l)(\mathbf{A}(l, l)a + p(l, l)) + \mathbf{H}(q)\lambda$ $\boldsymbol{\lambda}\geq \mathbf{0}$ $C(q)\ddot{q} + d(q, \dot{q}) \ge 0$ $0 \leq a \leq 1$

Trajectory Optimization

- •Modulates reference motion to
	- Reproduce original reference motion more accurately and robustly
	- Adapt to new conditions and requirements

Trajectory Optimization

- •Optimize foot trajectories only • Most essential components of fullbody gaits
	- Step locations is a key factor for balance

 \times 3 key frames

• Represented by

Trajectory Optimization

- •Objective
	- Pose difference
	- Falling down
	- Efficiency (consumed energy / move distance)
	- Contact force
	- Muscle force

•Covariance Matrix Adaptation

Motion Capture Reference

in-place slow run

Unilateral Painful Ankle Plantar Flexor

•People tend to reduce the use of the ankle plantar flexor.

•Minimizing muscle force of left ankle plantar flexor

Painful Joints on Unilateral Limb

•People tend to reduce contact force of the limb.

•Minimizing contact force of left limb

Painful Left Ankle Plantar Flexor Painful Joints on Left Leg

Bilateral *Gluteus Medius* & *Minimus* Weakness

•*Waddling gait* is observed for these people.

•Scaling maximum isometric force by 0.4

Unilateral *Gluteus Medius* & *Minimus* Weakness

•*Trendelenburg gait* is observed for these people.

•Scaling maximum isometric force by 0.2

Hamstrings, *Psoai*Tightness & Ankle Plantar Flexors Weakness

•Most common reason for *Crouch gait*

- •Scaling tendon slack length & maximum isometric force
	- by 0.8 (tightness) & by 0.2 (weakness), respectively

Unilateral Dislocation of Hip

•*Trendelenburg gait* is observed for these people.

• Moving left hip joint 3 cm in the lateral direction

80 N for 0.2 sec

Comparison with EMG data

*Reported by Demircan et al. [2009]

Discussion

- •First locomotion controller for "manymuscle" humanoids developed for clinical purpose.
- •Shows details of humanoids to reproduce various pathologic gait patterns

•Virtual surgical planning

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Locomotion Control for Many-Muscle Humanoids

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